



## Flow of Viscoelastic Fluid with Microrotation at a Boundary Layer Flow of a Horizontal Circular Cylinder

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### ABSTRACT

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In this study, the dynamics of the non-Newtonian viscoelastic fluid with microrotation at a boundary layer of a horizontal circular cylinder is investigated. For this case, Lorentz force is induced by external magnetic field positioned at right angle of the fluid flow, hence the magnetohydrodynamic effect is embedded in the momentum equation of the proposed model in addition to other governing parameters. The constitutive equations are converted to dimensionless form along with the associated boundary conditions before the resulting partial differential equations are solved using finite difference technique in Fortran programming. Results are validated before the velocity and microrotation profiles are examined and the effects of material, viscoelastic and magnetohydrodynamic parameter on the flow is discussed.

## 1. Introduction

The attribute of a fluid is the classification factor whether it belongs in Newtonian or non-Newtonian family. In simple terms, fluid that flows constantly without resistant at a certain temperature due to unchanged viscosity such as water and gasoline are Newtonian. Meanwhile, fluid which flow comes to a halt over time or gain momentum caused by altered viscosity when force is applied like cosmetics and asphalt belongs to the non-Newtonian family. The non-Newtonian fluid is a more complicated subject of study than Newtonian because it defies the Newton's law of viscosity. However, despite the complication, the study on non-Newtonian fluid is still sought-after due to numerous applications.

A theoretical and experimental study, for example, has been conducted by Mohamed and AbdelGawad [1] where they investigate the suitability of non-Newtonian fluid in medical application, namely for the broken bones bandage. The study accomplished to attest the aptness and capability of non-Newtonian fluid at reducing sudden impact for patient's safety and wellness. The application of non-Newtonian fluid also been discussed by Marinov [2] through modelling the work material as viscoplastic fluid where the result from the investigation can be used to analyze and interpret the

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phenomena in the metal cutting process. Besides that, non-Newtonian fluid is also important in pharmaceutical field. For instance, Thurston and Martin [3] have reviewed the behaviour of a polymeric solution called carboxymethylcellulose that is commonly used in drug product formulation using the generalized Maxwell model. Different models are used in different studies to represent the flow of different type on fluids depending on the dominant characteristics of the fluid itself.

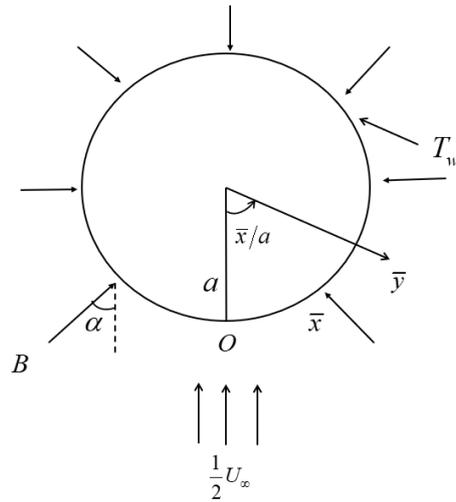
This study will explore the model for the flow of viscoelastic fluid with microrotation. Viscoelastic fluid is viscous fluid with an extra distinct feature of elasticity. There are varieties of model for viscoelastic fluid documented and the simplest model that could portray the viscous and elastic nature of the fluid is the Maxwell model that has been addressed by Brujan [4]. The extension of the prior model is the Oldroyd-B model which takes into consideration the rate of deformation tensor and can be reduced to Maxwell model when the retardation parameter is set to 0. Aside from these, there is also the Dumbbell model that can be further divided into another two models, namely the elastic dumbbell and rigid dumbbell model. Lastly, there is the BKBZ model which is the integral type of constitutive equations. Among the study that considers these models to represent the flow of viscoelastic fluid for the case of bluff body have been presented by several authors [5-8].

Besides being viscoelastic in nature, the fluid in interest in this study contains microelements that according to Karvelas *et al.*, [9] have varying size and shape, that rotate and move independently of the bulk flow, detached from the flow and rotation of the fluid. Micropolar fluid theory introduced by Eringen [10] is the fittest model to portray the characteristics of these microelements that are suspended in viscous fluid. There are substantial number of literatures on micropolar fluid model but only a handful deliberated on the flow characteristics of micropolar fluid over bluff body. The case of micropolar flow past circular cylinder has been discussed in detail in a number of studies [11-13]. While other studies have highlighted the dynamics of the flow when the geometry involved is sphere [14-16].

However, in this study, an elastic fluid that contains suspended microelements that are in the form of short, rigid, dumb-bell molecule such as blood and liquid crystal elastomers is considered. In order to mimic the characteristics of the fluid to the utmost, both parameters from viscoelastic and micropolar model are linked in a set of constitutive equations for an improvised viscoelastic micropolar model. It is also of interest to see the change in the flow of the fluid when it is exposed to a magnetic field inclined at an angle. The investigation on MHD effect on viscoelastic fluid has been presented by Kasim *et al.*, [17] and Mahat *et al.*, [18] while Bhat and Katagi [19] has examined the MHD effect on micropolar fluid flow. Both studies have demonstrated that magnetic effect does exist on the flow. The study of magneto-convective viscoelastic micropolar has been discussed by Aziz *et al.*, [20] but this study will put more focus on the flow itself in terms of the velocity and boundary layer separation without consideration of the heat transfer process.

## 2. Mathematical Formulation

An incompressible two-dimensional flow of a horizontal circular cylinder with radius  $a$ , submerged in a viscoelastic micropolar fluid while imposed to a magnetic field acting at an inclined angle is the subject of this research. This problem is investigated under the assumption that the temperature for the surface of the cylinder remains constant. The illustration of the model is shown in Figure 1 where  $s$  is the circumference measurement of the cylinder from the lower stagnation point while  $r$  represents the length perpendicular to the body surface and  $U_\infty$  is the free stream velocity.



**Fig. 1.** Schematic diagram for the flow

The problem is governed by a set of equations that each represents the characteristics of the flow as follows:

$$\frac{\partial \bar{u}}{\partial \bar{x}} + \frac{\partial \bar{v}}{\partial \bar{y}} = 0 \quad (1)$$

$$\bar{u} \frac{\partial \bar{u}}{\partial \bar{x}} + \bar{v} \frac{\partial \bar{u}}{\partial \bar{y}} = \bar{u}_e \frac{d\bar{u}_e}{d\bar{x}} + \left( \frac{\mu + \kappa}{\rho} \right) \frac{\partial^2 \bar{u}}{\partial \bar{y}^2} + \frac{\kappa}{\rho} \frac{\partial \bar{N}}{\partial \bar{y}} + \frac{k_0}{\rho} \left[ \frac{\partial}{\partial \bar{x}} \left( \bar{u} \frac{\partial^2 \bar{u}}{\partial \bar{y}^2} \right) + \bar{v} \frac{\partial^3 \bar{u}}{\partial \bar{y}^3} - \frac{\partial \bar{u}}{\partial \bar{y}} \frac{\partial^2 \bar{u}}{\partial \bar{x} \partial \bar{y}} \right] \quad (2)$$

$$-\frac{\sigma}{\rho} (\bar{u} - \bar{u}_e) B_0^2 \sin^2 \alpha_1$$

$$\rho j \left( \bar{u} \frac{\partial \bar{N}}{\partial \bar{x}} + \bar{v} \frac{\partial \bar{N}}{\partial \bar{y}} \right) = -\kappa \left( 2\bar{N} + \frac{\partial \bar{u}}{\partial \bar{y}} \right) + \gamma \frac{\partial^2 \bar{N}}{\partial \bar{y}^2} \quad (3)$$

The boundary conditions associated to the governing equations are

$$\bar{u} = \bar{v} = 0, \quad \bar{N} = -n \frac{\partial \bar{u}}{\partial \bar{y}} \quad \text{on } \bar{y} = 0, \quad (4)$$

$$\bar{u} \rightarrow \bar{u}_e(x), \quad \frac{\partial \bar{u}}{\partial \bar{y}} \rightarrow 0, \quad \bar{N} \rightarrow 0, \quad \text{as } \bar{y} \rightarrow \infty$$

Each parameter that made up the equations represents different physical quantities with different units which justifies the reason why non-dimensionalisation is necessary as the next step. These variables are introduced

$$x = \frac{\bar{x}}{a}, \quad y = \frac{\text{Re}^{1/2} \bar{y}}{a}, \quad u = \frac{\bar{u}}{U_\infty}, \quad v = \frac{\text{Re}^{1/2} \bar{v}}{U_\infty}, \quad N = \frac{\text{Re}^{-1/2} a \bar{N}}{U_\infty}, \quad u_e = \frac{\bar{u}_e(\bar{x})}{U_\infty} \quad (5)$$

resulting to the following set of dimensionless equations.

$$\frac{\partial u}{\partial x} + \frac{\partial v}{\partial y} = 0 \quad (6)$$

$$u \frac{\partial u}{\partial x} + v \frac{\partial u}{\partial y} = u_e \frac{du_e}{dx} (1 + K_1) \frac{\partial^2 u}{\partial y^2} + K_1 \frac{\partial N}{\partial y} + K \left[ \frac{\partial}{\partial x} \left( \bar{u} \frac{\partial^2 \bar{u}}{\partial y^2} \right) + \bar{v} \frac{\partial^3 \bar{u}}{\partial y^3} - \frac{\partial \bar{u}}{\partial y} \frac{\partial^2 \bar{u}}{\partial x \partial y} \right] - M (u - u_e) \sin^2 \alpha_1 \quad (7)$$

$$u \frac{\partial N}{\partial x} + v \frac{\partial N}{\partial y} = -K_1 \left( 2N + \frac{\partial u}{\partial y} \right) + \left( 1 + \frac{K_1}{2} \right) \frac{\partial^2 N}{\partial y^2} \quad (8)$$

subjected to the boundary conditions

$$u = v = 0, \quad N = -n \frac{\partial u}{\partial y} \quad \text{on } y = 0 \quad (9)$$

$$u \rightarrow u_e(x), \quad \frac{\partial u}{\partial y} \rightarrow 0, \quad N \rightarrow 0 \quad \text{as } y \rightarrow \infty$$

The main parameters in the constitutive equations, which are the viscoelastic parameter,  $K$ , the material parameter,  $K_1$ , magnetic parameter,  $M$  as well as the microinertia density,  $j$ , and the spin gradient viscosity, can be defined as

$$K = \frac{k_0 U_\infty}{a \rho \nu}, \quad K_1 = \frac{\kappa}{\mu}, \quad M = \frac{\sigma B_0^2 a}{\rho U_\infty}, \quad j = \frac{a \nu}{U_\infty}, \quad \gamma = \left( \mu + \frac{\kappa}{2} \right) j \quad (10)$$

Then, the following set of similarity equations is introduced to simplify the equations by reducing the dependence of some terms to a single variable instead of two. The variables that follow are assumed to solve Eq. (6) to Eq. (8) subjected to the boundary conditions in Eq. (9).

$$\psi = x f(x, y), \quad N = x g(x, y) \quad (11)$$

where the stream function, is defined as

$$u = \frac{\partial \psi}{\partial y}, \quad v = -\frac{\partial \psi}{\partial x} \quad (12)$$

As a result from the transformation, these equations are obtained.

$$(1 + K_1) \frac{\partial^3 f}{\partial y^3} + f \frac{\partial^2 f}{\partial y^2} - \left( \frac{\partial f}{\partial y} \right)^2 + \frac{\sin x \cos x}{x} + K_1 \frac{\partial g}{\partial y} - M \left( \frac{\partial f}{\partial y} - \frac{\sin x}{x} \right) \sin^2 \alpha$$

$$+ K \left\{ 2 \frac{\partial f}{\partial y} \frac{\partial^3 f}{\partial y^3} - f \frac{\partial^4 f}{\partial y^4} - \left( \frac{\partial^2 f}{\partial y^2} \right)^2 + x \left( \frac{\partial^2 f}{\partial x \partial y} \frac{\partial^3 f}{\partial y^3} - \frac{\partial f}{\partial x} \frac{\partial^4 f}{\partial y^4} + \frac{\partial f}{\partial y} \frac{\partial^4 f}{\partial x \partial y^3} - \frac{\partial^2 f}{\partial y^2} \frac{\partial^3 f}{\partial x \partial y^2} \right) \right\} \quad (13)$$

$$= x \left( \frac{\partial f}{\partial y} \frac{\partial^2 f}{\partial x \partial y} - \frac{\partial f}{\partial x} \frac{\partial^2 f}{\partial y^2} \right)$$

$$\left(1 + \frac{K_1}{2}\right) \frac{\partial^2 g}{\partial y^2} + f \frac{\partial g}{\partial y} - g \frac{\partial f}{\partial y} - K_1 \left(2g + \frac{\partial^2 f}{\partial y^2}\right) = x \left(\frac{\partial f}{\partial y} \frac{\partial g}{\partial x} - \frac{\partial f}{\partial x} \frac{\partial g}{\partial y}\right) \quad (14)$$

bounded by the transformed boundary conditions

$$f = \frac{\partial f}{\partial y} = 0, \quad g = -\frac{1}{2} \frac{\partial^2 f}{\partial y^2} \quad \text{at } y = 0$$

$$\frac{\partial f}{\partial y} = \frac{\sin x}{x}, \quad \frac{\partial^2 f}{\partial y^2} = 0, \quad g = 0 \quad \text{as } y \rightarrow \infty \quad (15)$$

The value  $n=1/2$  is chosen for this problem where it indicates weak concentration in microelements and rotation is plausible, while the anti-symmetric part of the stress tensor is vanishing [21]. At the lower stagnation point of the cylinder, the constitutive equations of the viscoelastic micropolar flow are reduced to a set of differential equation given by

$$(1 + K_1) f''' + ff'' - f'^2 + 1 + K_1 g' - M (f' - 1) \sin^2 \alpha + K (2f' f''' - f f^{iv} - f''^2) = 0 \quad (16)$$

$$\left(1 + \frac{K_1}{2}\right) g'' + fg' - f'g - K_1 (2g + f'') = 0 \quad (17)$$

corresponds to the boundary conditions

$$f(0) = f'(0) = 0, \quad g(0) = -\frac{1}{2} f''(0) \quad \text{at } y = 0$$

$$f'(\infty) = 1, \quad f''(\infty) = 0, \quad g(\infty) = 0 \quad \text{as } y \rightarrow \infty \quad (18)$$

where the derivatives are with respect to  $y$  variable.

### 3. Results and Discussion

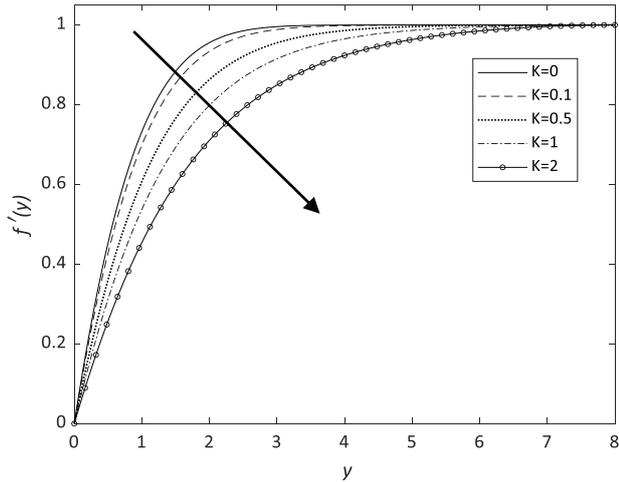
The numerical solutions for the non-Newtonian flow model are attained by using the Keller-box method in Fortran programming. For verification purpose, the results obtained are compared to the exact solution from Ariel [22] and numerical solution from another limiting case of viscoelastic model by Anwar *et al.*, [23]. The comparison of the resulting skin friction values for a variety of viscoelastic parameter values to the mentioned literatures is presented in Table 1. Considering the commendable degree of similarity between the current result and the exact solution, it is decent to proclaim that the current model is trustworthy.

**Table 1**  
 Values of  $f''(0)$  at different values of  $K$  when  $M=K_1=0$

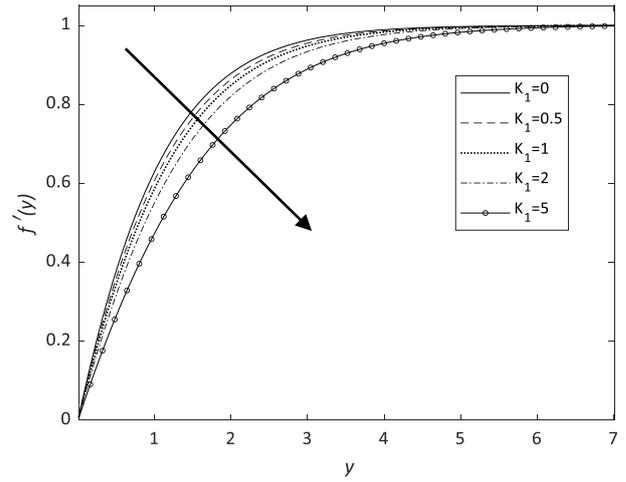
$K$	Exact solution (Ariel [22])	Present	Viscoelastic model (Anwar <i>et al.</i> , [23])
0	1.232588	1.232657	-
0.01	-	1.221447	1.222693
0.05	1.179830	1.179893	-
0.1	1.134114	1.134172	1.135982
0.2	1.058131	1.058180	1.045412
0.3	0.996844	0.996886	0.960922
0.4	0.945869	0.945907	0.882512
0.5	0.902500	0.902535	0.810182
0.6	-	0.864985	0.743933
0.7	-	0.832019	0.683763
0.8	-	0.802749	0.629673
0.9	-	0.776511	0.581664
1	0.752766	0.752803	-
100	0.099515	0.100783	-
500	0.044677	0.045487	-
1000	0.031607	0.032229	-

Figure 2, Figure 3 and Figure 4 show the velocity profiles of the flow when the different values of viscoelastic, material and magnetic parameters are considered. The result reveals that a rise in the values of viscoelastic and material parameter lead to reduction in the velocity profile while the elevation of magnetic parameter enhanced the velocity of the flow. From the result, it appears that the MHD effects may boost the velocity of viscoelastic micropolar fluid and since only positive values are recorded, it means that there is no reversal flows for the selected values of magnetic parameter. From Figure 7, it is evident that the Lorentz force formed when the electrically conducting fluid moves through the induced magnetic field affect the skin friction, which in turns delay the undesirable boundary layer separation as the magnetic parameter increases.

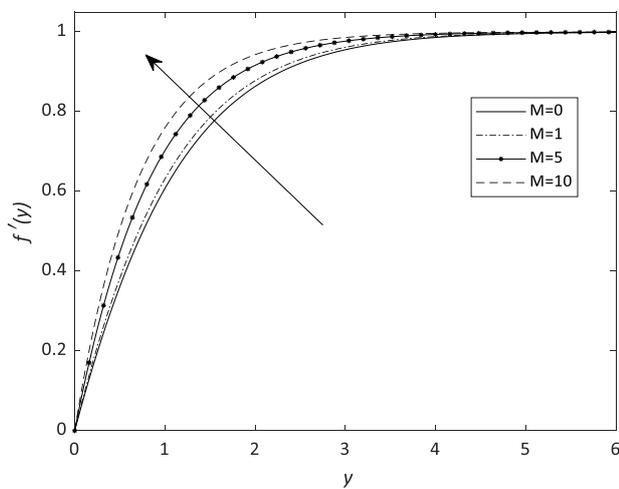
It can be observed from Figure 3 that higher number of macro particles in the fluid hinder the fluid movement, causing the velocity to reduce while Figure 6 suggests that high concentrated mass in the flow downscale the effect of skin friction on the cylinder surface. As for the viscoelasticity effect, being highly viscoelastic can retard the flow of fluid as well as procrastinate the separation. Similar result has been documented by Jones and Lewis [24] when they investigate the separation phenomenon for the flow past a cylinder. The study concludes that viscoelasticity causes the point of separation to move towards the front stagnation point.



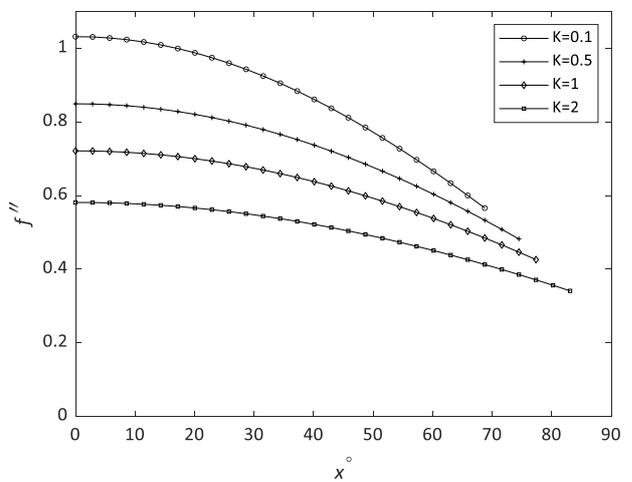
**Fig. 2.** Velocity profile at various  $K$  values



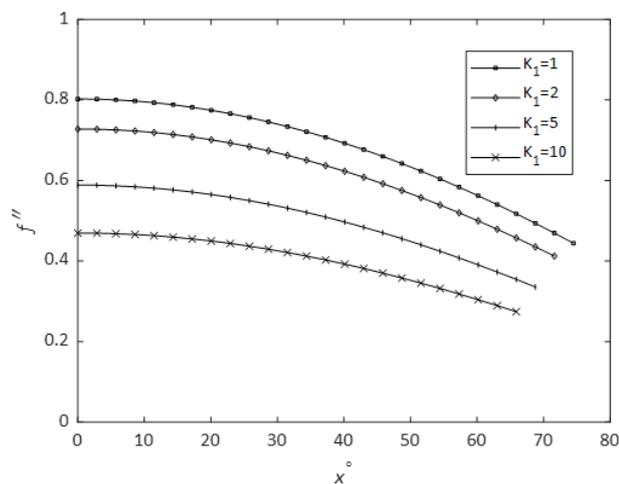
**Fig. 3.** Velocity profile at various  $K_1$  values



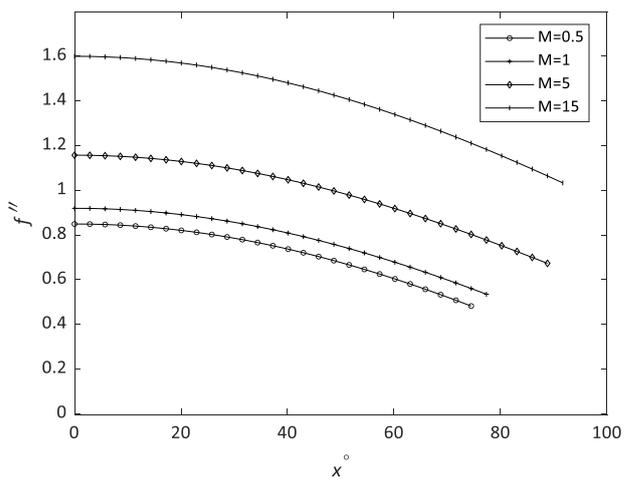
**Fig. 4.** Velocity profile at various  $M$  values



**Fig. 5.** Skin friction coefficient at various  $K$  values



**Fig. 6.** Skin friction coefficient at various  $K_1$  values



**Fig. 7.** Skin friction coefficient at various  $M$  values

#### 4. Conclusions

The problem of boundary layer flow of viscoelastic micropolar fluid with aligned MHD effect is investigated. Holding other parameters constant, the results obtained suggested that:

- I. higher viscoelastic parameter will result in higher velocity and decrease the skin friction coefficient.
- II. rise in the value of magnetic parameter boost the velocity as well as the skin friction coefficient.
- III. when the material parameter increases, both velocity and skin friction coefficient decrease.
- IV. boundary layer separation is delayed for greater values of magnetic and viscoelastic parameter, but lower value of material parameter.

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